

# Functionalized surfaces for the detection of circulating tumor cells (CTC) and bacteria

## 2- Surface functionalization strategies for CTC detection and analysis

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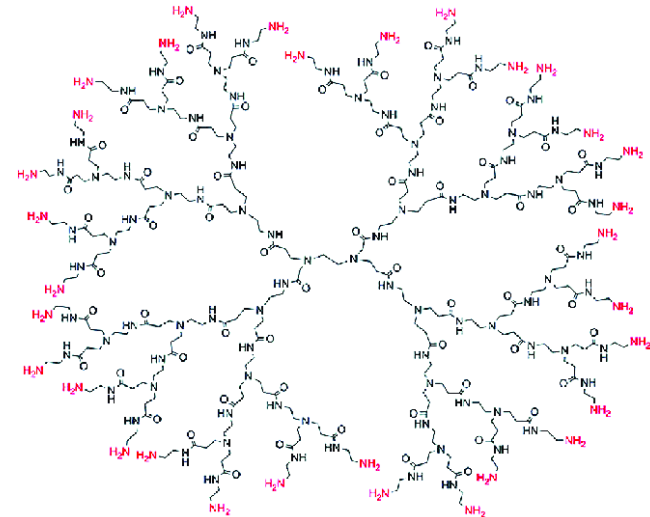
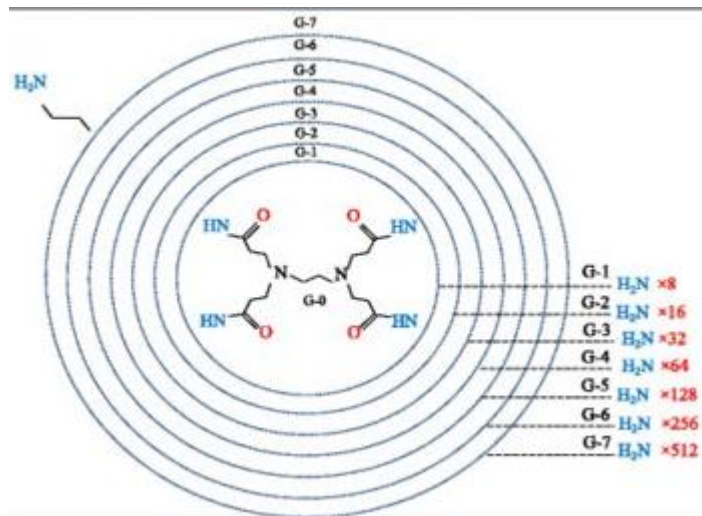
# Challenges for CTC detection

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- ☞ The discovery of CTC as a liquid biopsy had a revolutionary effect on early diagnosis, metastasis detection and personalized tumor treatment
  - ☒ Use to detect the biological characteristic and molecular type of primary tumor cells
  - ☒ Understanding their part in the metastasis may contribute to better therapeutic management
  
- ☞ Challenges:
  - ☒ Rare: 1-100 CTC with  $10^6$ - $10^8$  RBC /mL
  - ☒ Heterogenous with variation in the expression of surface biomarkers
  - ☒ Non destructive capture and detection methods for subsequent analysis : image analysis, cell culture, drug screening
  
- ☞ Selective capture of all CTC
  
- ☞ Release from surfaces without damaging the target cells
  
- ☞ Detection method for infinitesimally concentration in the blood stream

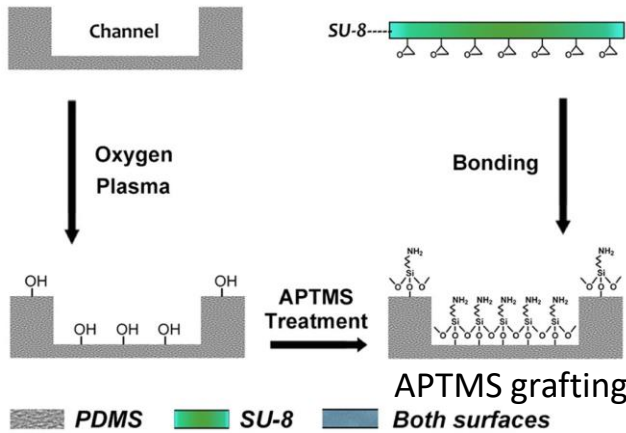
# Non fouling surfaces

- ☞ One major problem for CTC detection device: non specific adsorption
  - ☒ depends on hydrophilicity/hydrophobicity of the surface
    - optimal water contact angle for cell adhesion between 60° and 80°
  - ☒ depends on charge of the surface
  - ☒ depends on roughness of the surface
- ☞ grafting of dendrimers amino-terminated or carboxylated-terminated

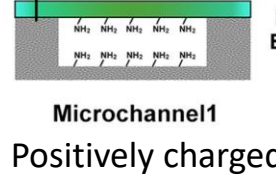
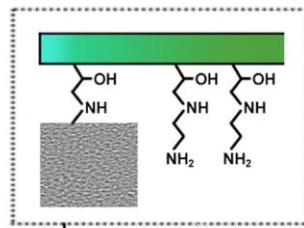


PANAM-NH<sub>2</sub> G3

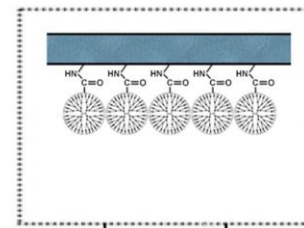
150µm x 50µm



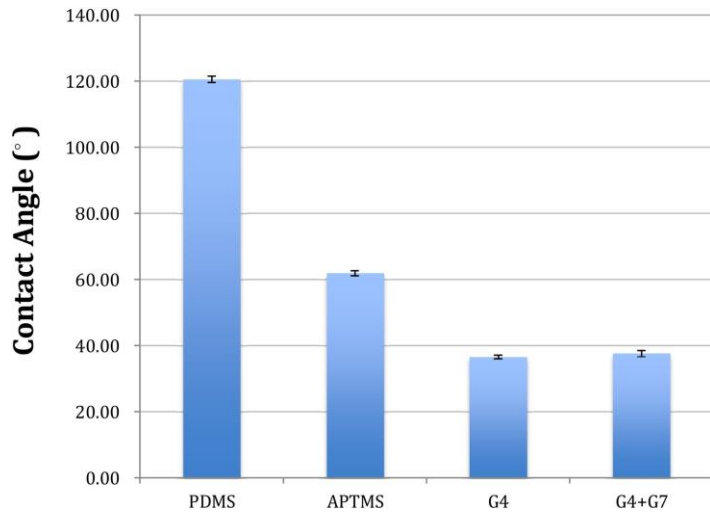
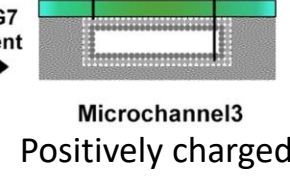
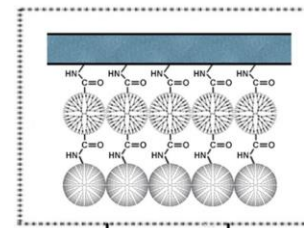
EDA grafting



PAMAM-COOH G4 grafting



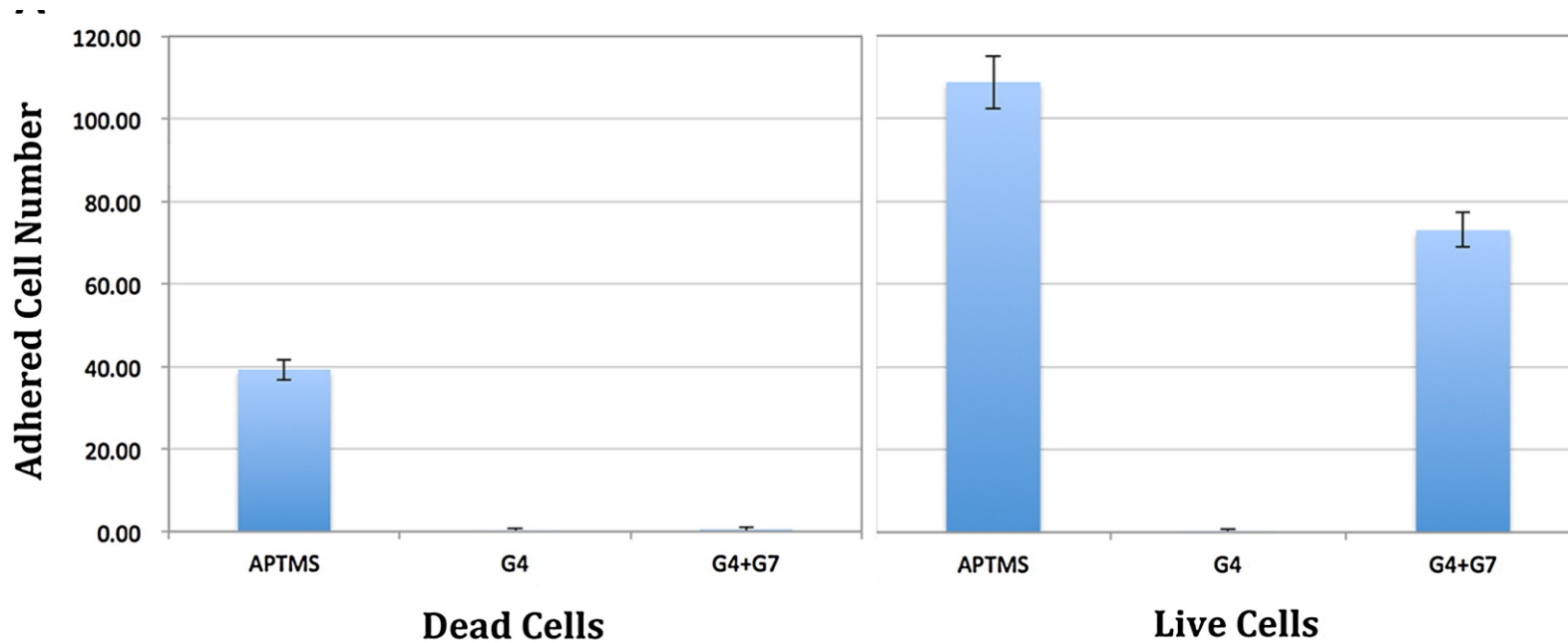
PAMAM-NH<sub>2</sub> G7 grafting



Qin et al., Colloids and Surfaces B 2017

Groups	AFM 3D Image	Vertical View	Roughness
Unmodified PDMS			0.26±0.04
PDMS with APTMS			1.19±0.06
G4			3.62±0.23
G4+G7			5.88±0.33

Injection of  $10^6$  CCRF-CEM cells/mL in PBS at 0.05 mL/h for 1h

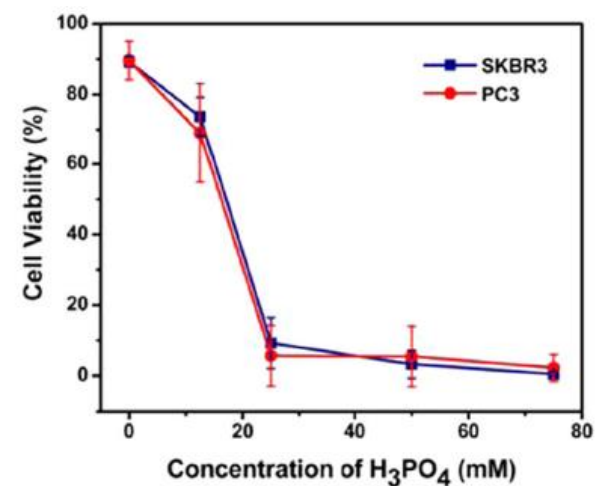
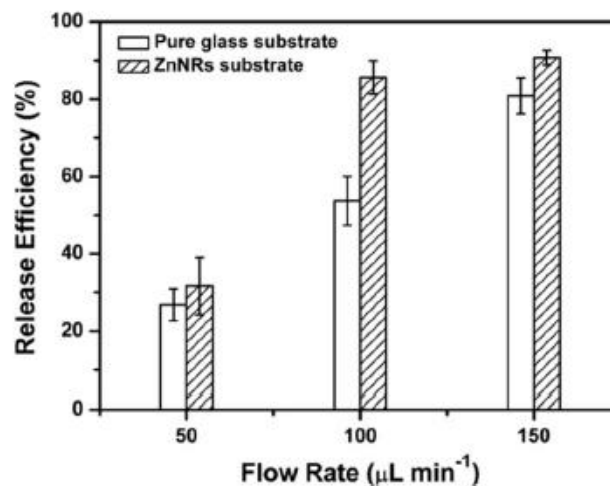
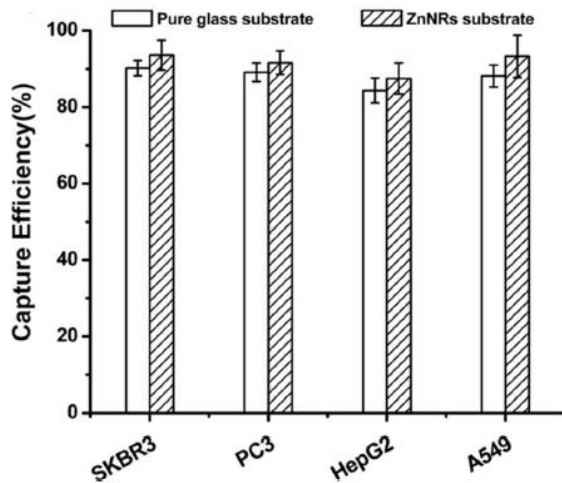
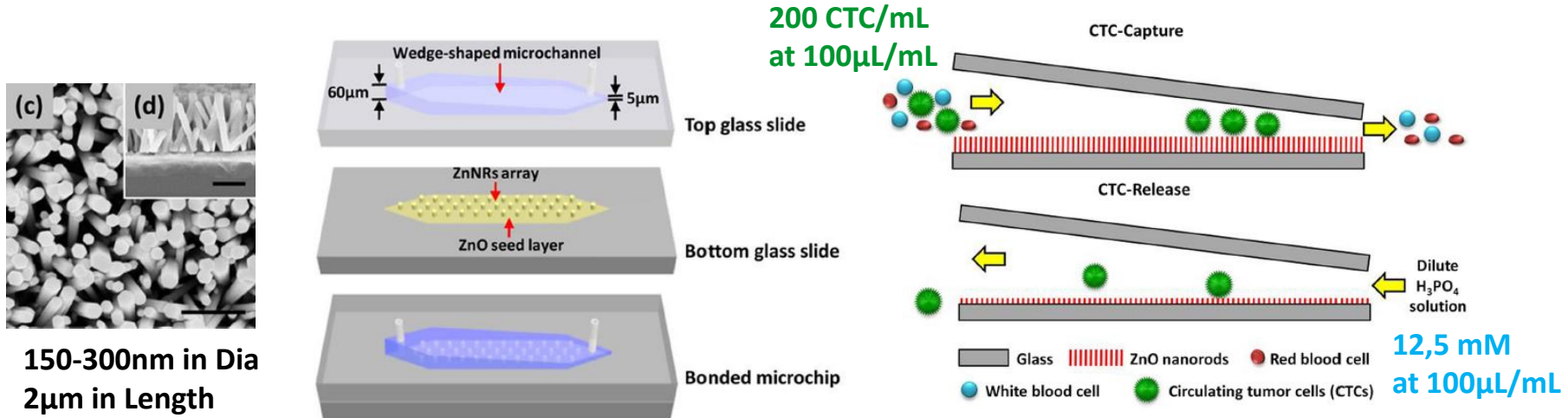


☒ Dead cells have no charge, Live cells are negatively charged

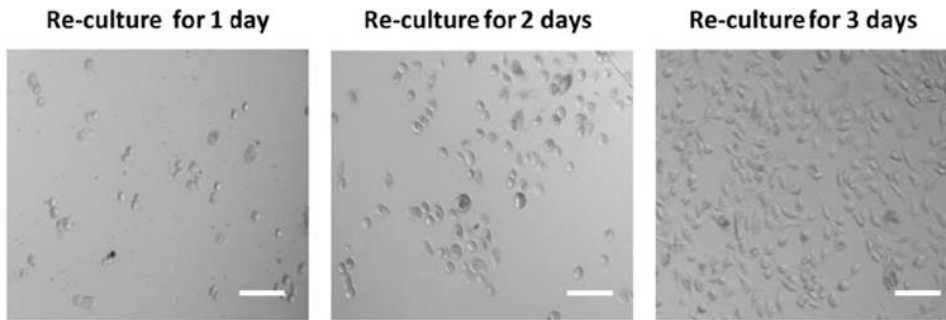
☞ Higher influence of charge surface than roughness or hydrophilicity  
(Tests done in PBS only)

# Implementation of nanomaterials with microfluidic

Microchip with ZnO nanorods on glass slide to capture and release CTC



Li et al., Biomed Microdevices 2017



- CTC capture efficiency  $\approx 85\%$
- CTC release efficiency  $\approx 85\%$
- CTC viability at 1 day  $\approx 70\%$
- CTC viability at 3 days  $\approx 90\%$

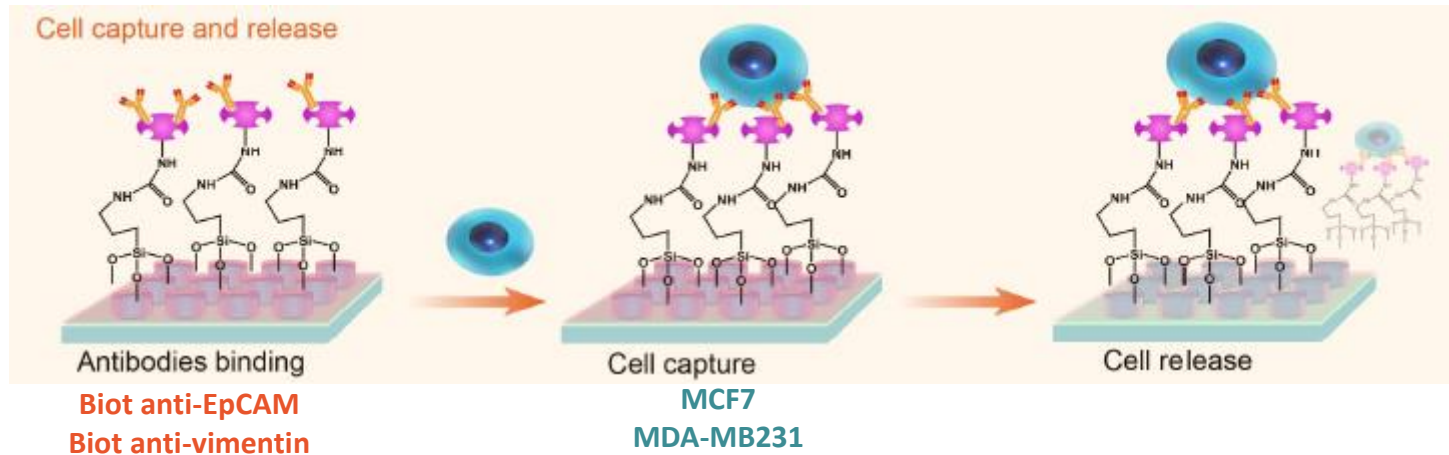
☞ What about CTC integrity?

☞ PDMS-based microfluidic chip with ZnO nanograss

80 $\mu\text{m}$  high  
160 $\mu\text{m}$  Dia  
260 $\mu\text{m}$  center-  
center pillar dist

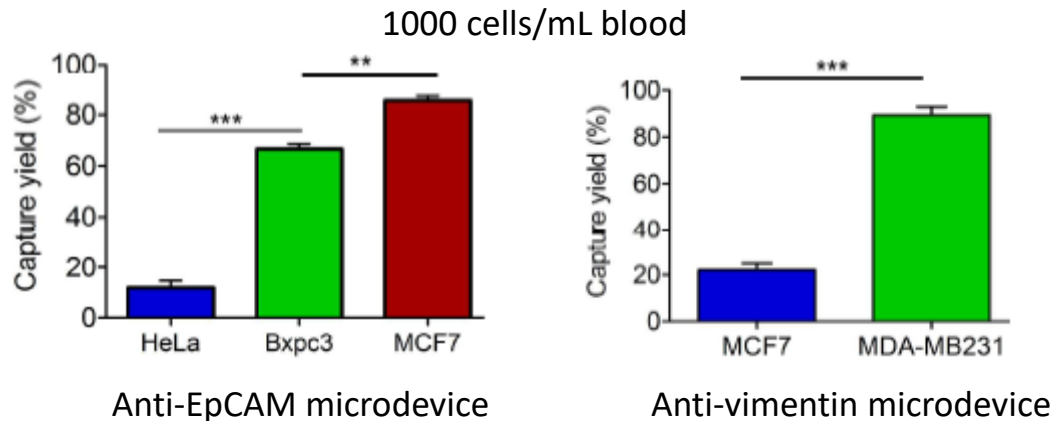


Hui et al., ACS Appl. Mater. Interfaces 2017



☒ ZnO nanogras reduce non specific adsorption of WBC

☞ EpCAM is epithelial cell biomarker; Vimentin is mesenchymal cell biomarker

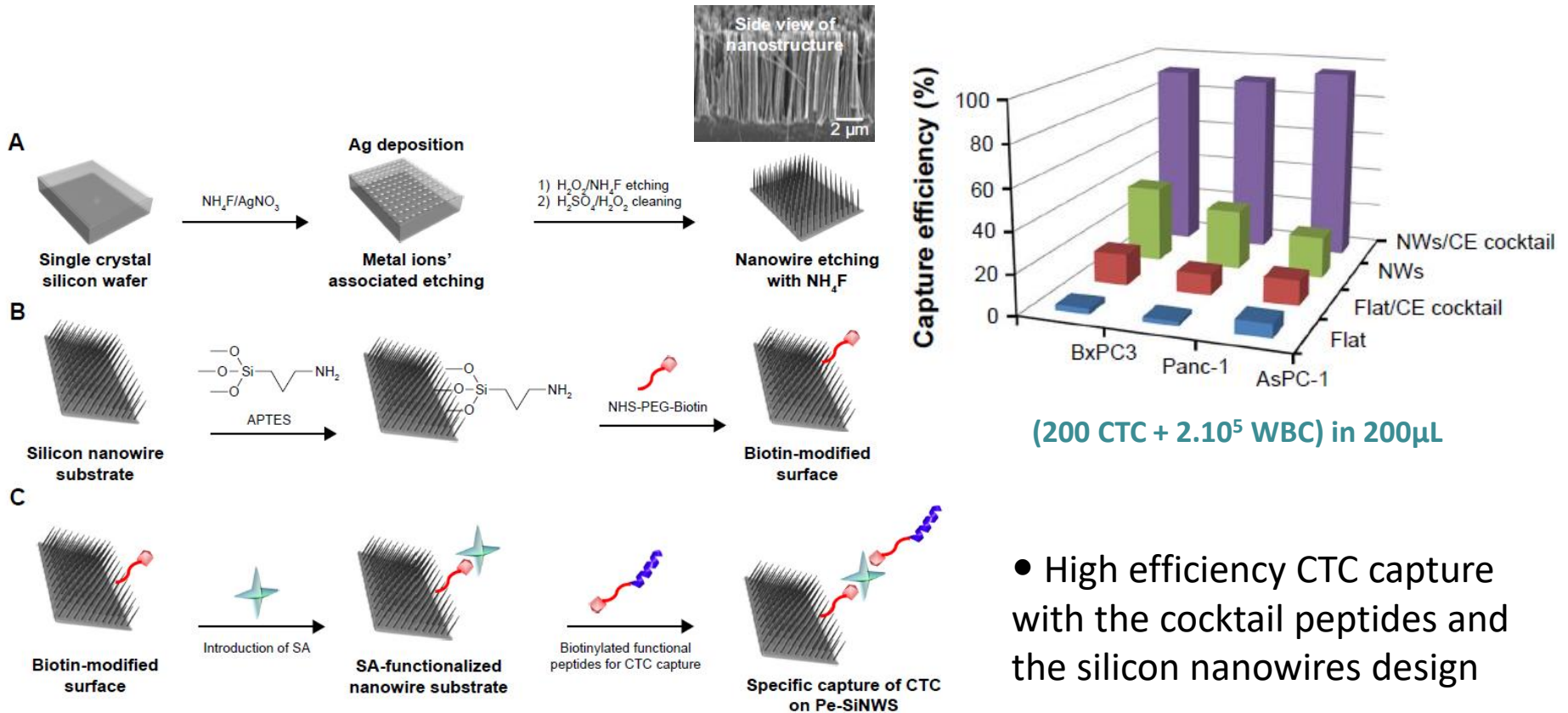


- Possibility to detach CTC from antibody functionalized ZnO nanogras by applying 0,1M HCl solution (pH5,6) with cell viability of 90%



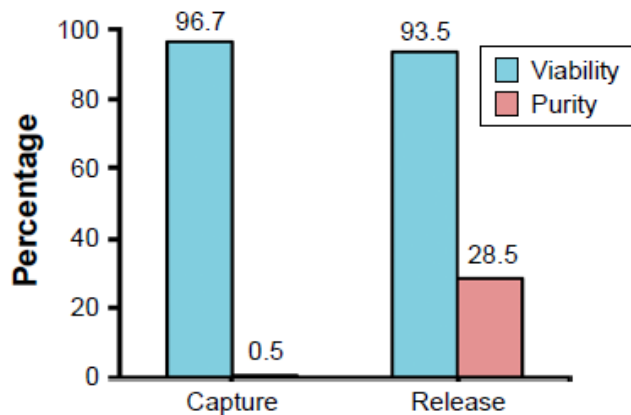
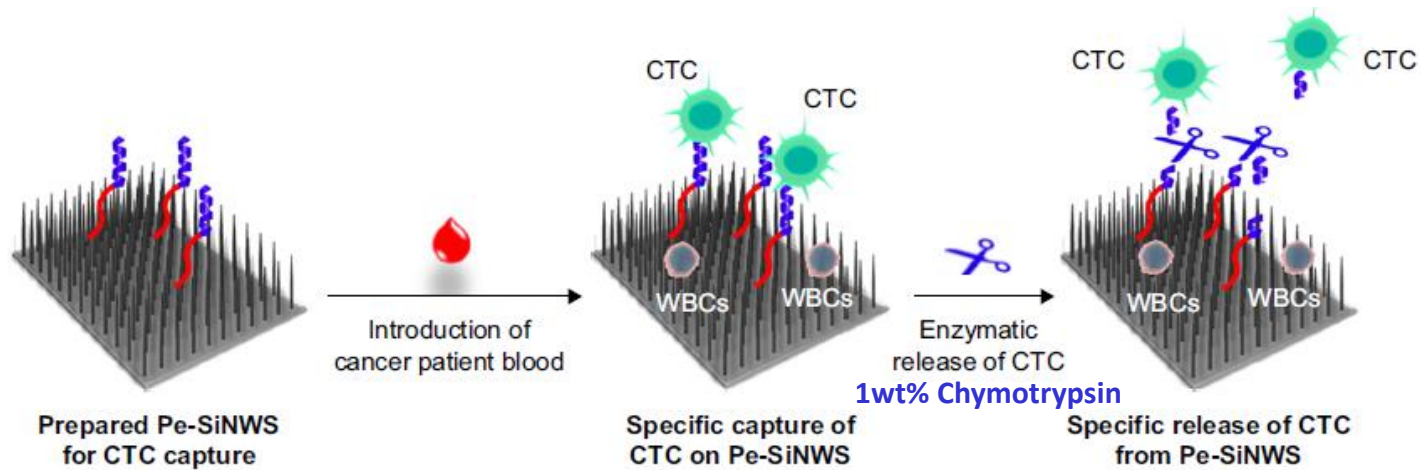
☞ Improve pancreatic CTC capture efficiency by combining 2 specific interactions with microfluidic device

- ☒ EpCAM positive CTC with EpCAM recognition peptide (Pep)
- ☒ EpCAM negative CTC with CKAANK peptide specific for pancreatic cancer cell



- High efficiency CTC capture with the cocktail peptides and the silicon nanowires design

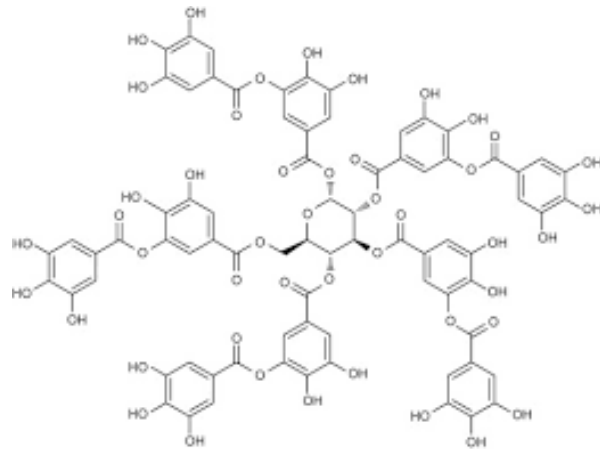
Shen et al., International J. Nanomedicine 2019



- Very good efficiency of CTC capture and release
- Very good CTC viability
- But very bad purity rate due to WBC non specific adsorption onto Si nanowires!

# Functionalization with chemical target of CTC membrane receptor

## ☞ Tannic acid on magnetic nanoparticles (MNP)



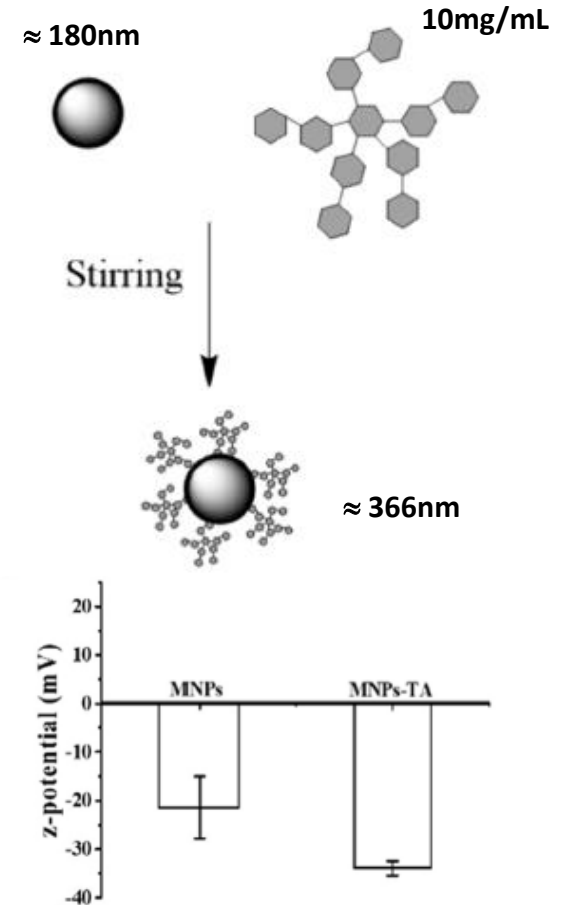
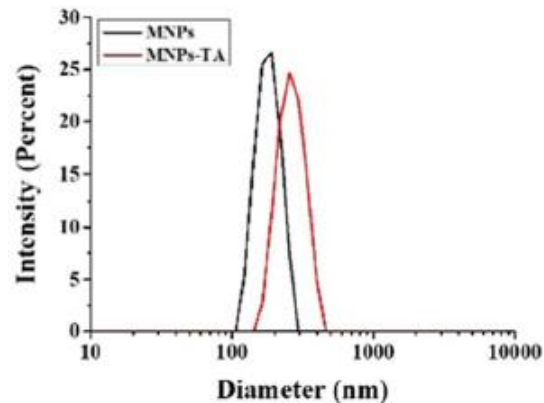
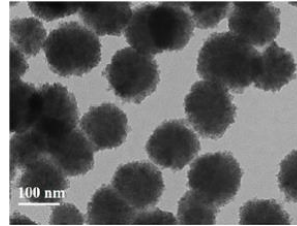
Tannic acid (TA)



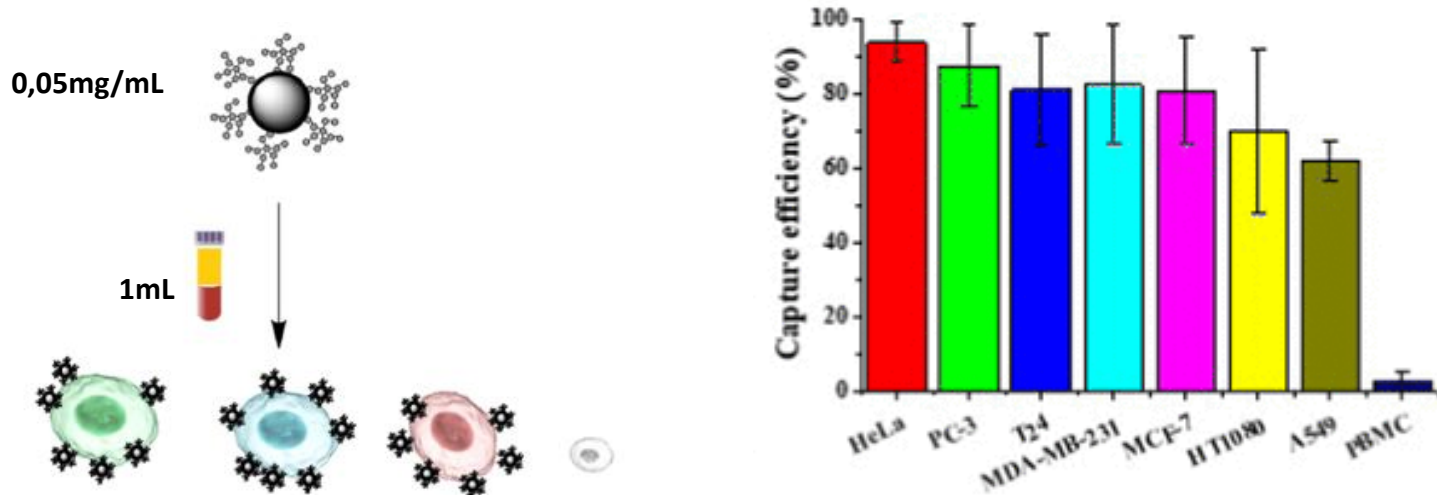
- Interact with K residues of PKM2
- Anti-adhesion effect on WBC

☒ FTIR analysis and UV-Vis spectra confirm the coupling of TA on Fe<sub>2</sub>O<sub>3</sub> MNP

MNP = FeCl<sub>3</sub> + PEG4000



Ding et al., ASC Appl. Mater. Interfaces 2021

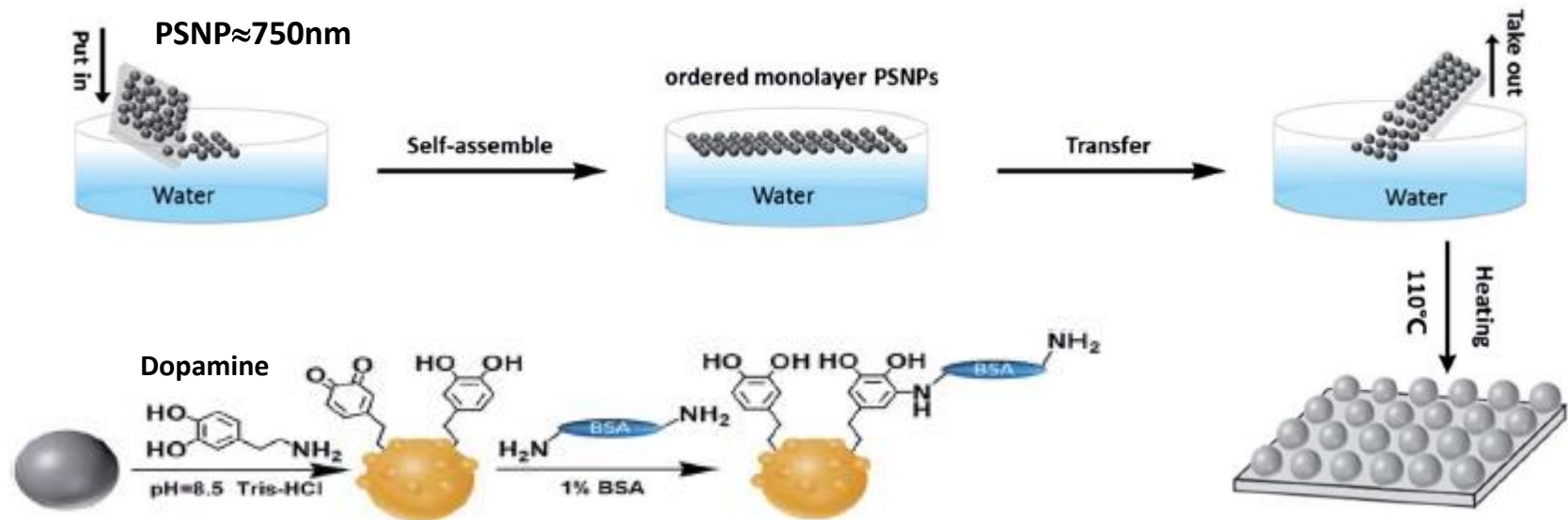


- 62-93% capture efficiency on 7 cancer cell lines

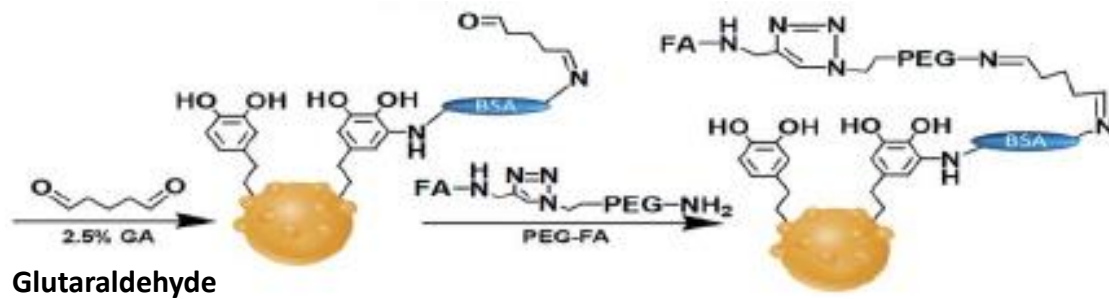
☞ CTC count in clinical samples:

- ☒ 21 cancer patients (8 type of cancers): from 1 to 10 CTC detected in 1mL blood
- ☒ 6 healthy donors: no CTC detected

## ☞ Folic acid on polystyrene nanosphere (PSNP)

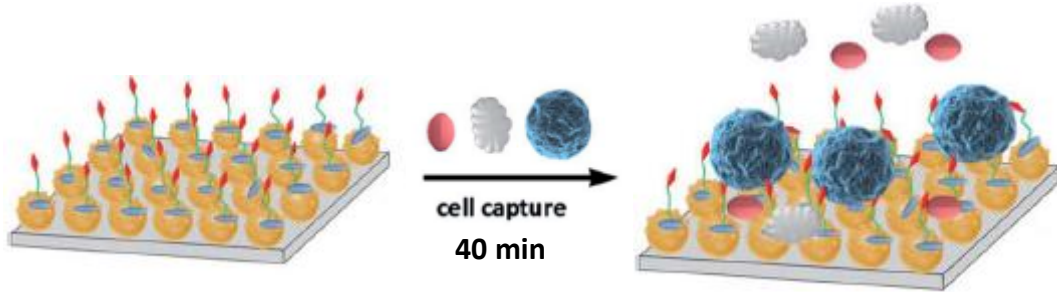


- reduction of non specific adsorption with BSA coupling

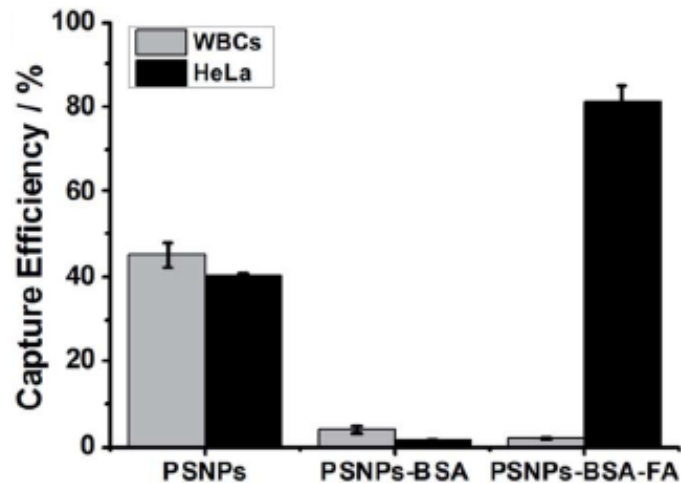
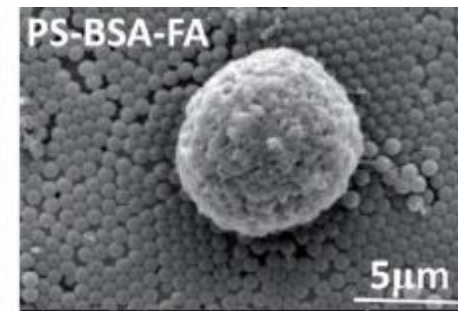
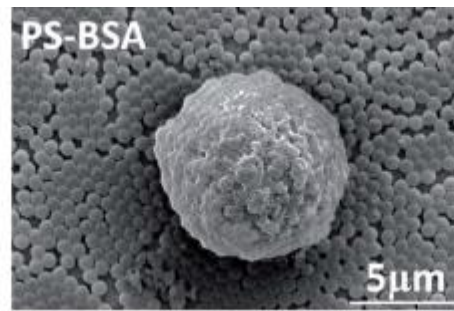
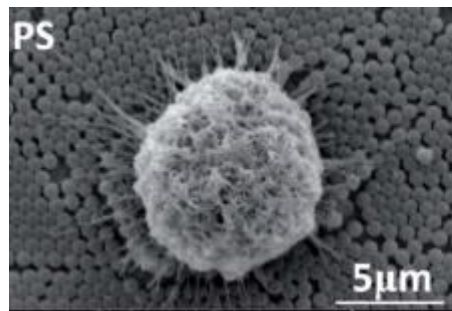


- FA-PEG-NH<sub>2</sub> obtained through click chemistry and characterized with <sup>1</sup>H NMR

Chen et al., Anal. Methods 2019

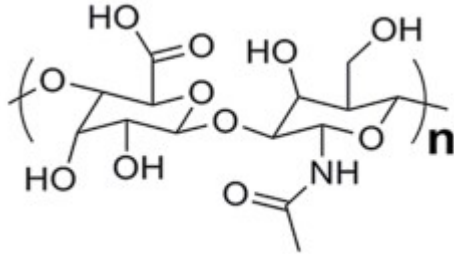


From 10 to 200 cell/mL



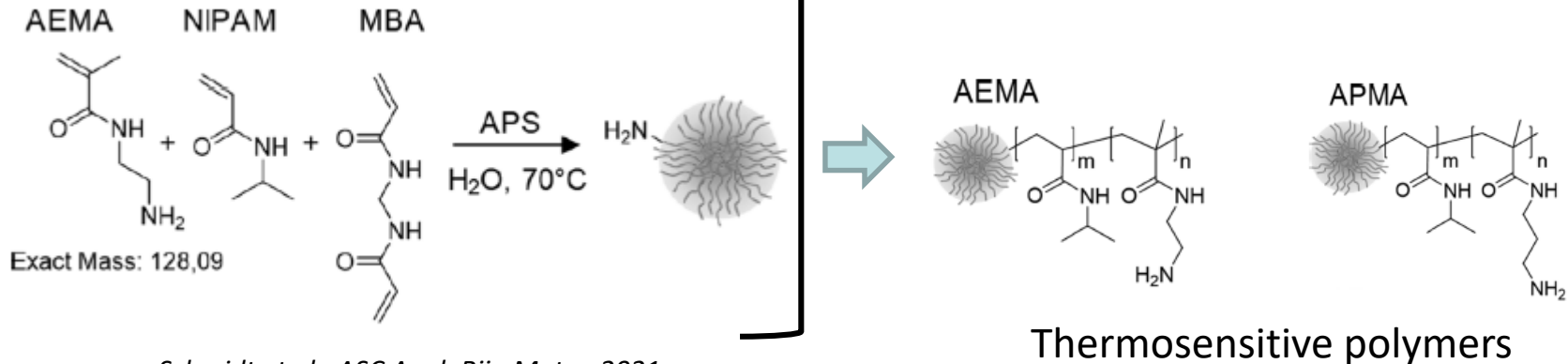
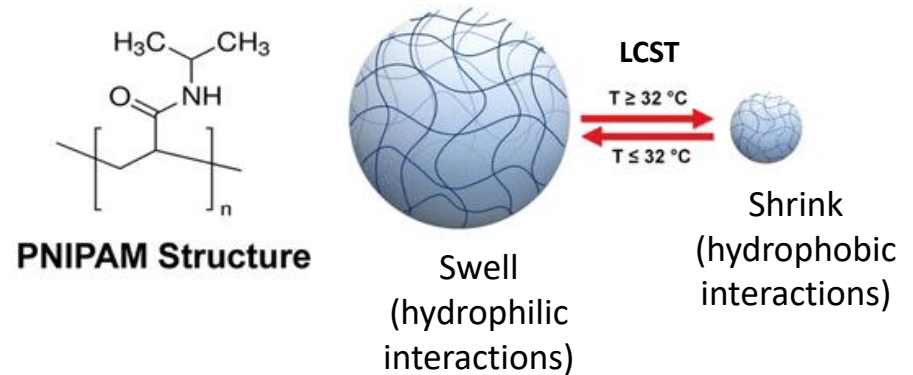
- FA-PSNP efficiently capture HeLa cell from (WBC + HeLa cell) sample
- Efficiency decrease to 40% in blood sample

## ☞ Hyaluronic acid (HA)-based microgel

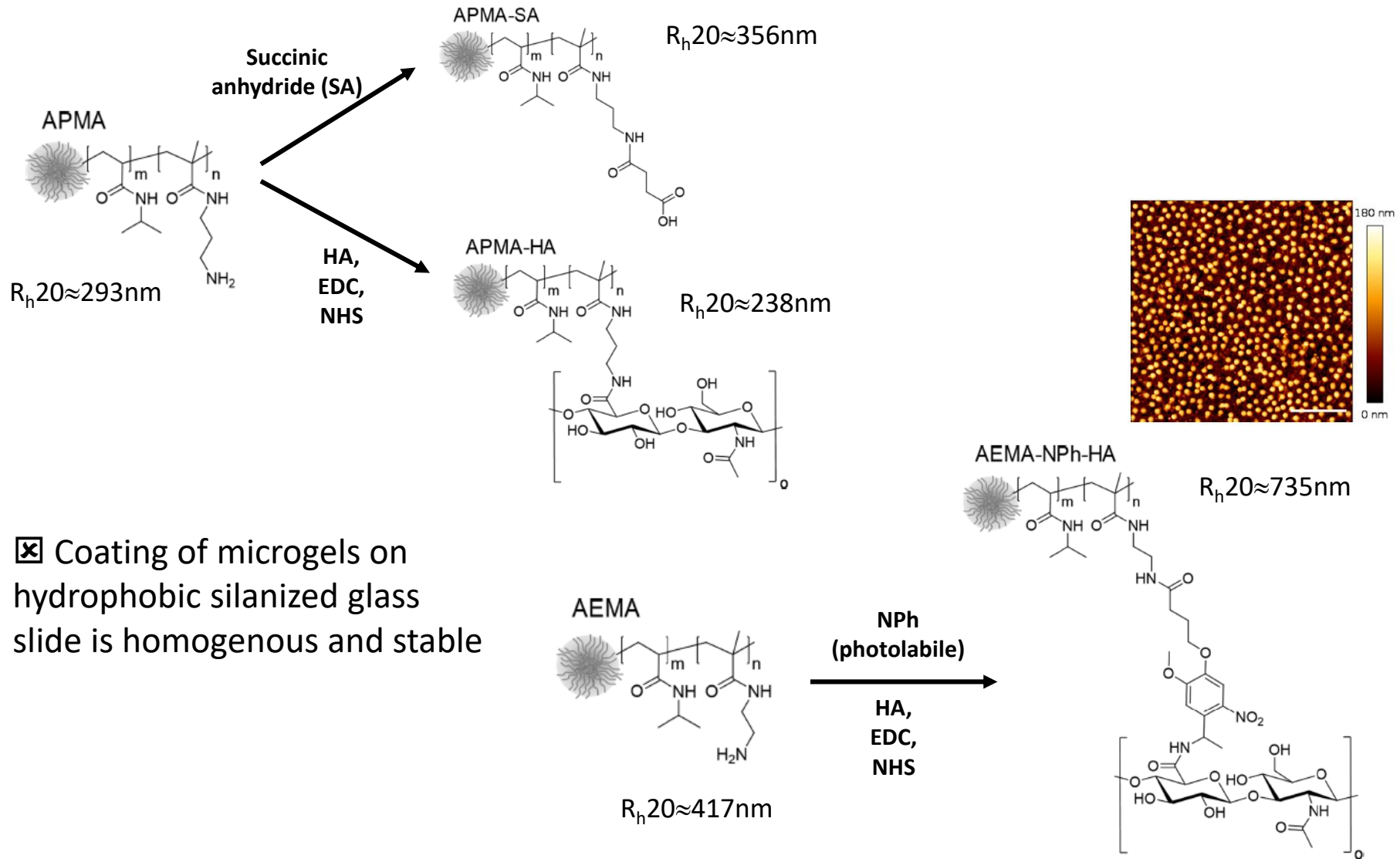


☒ HA is a glycan of ECM, known to promote tumor growth through interaction with CD44 cell receptor

☒ PNIPAM (poly(N-isopropylacrylamide)) is a thermoresponsive polymer

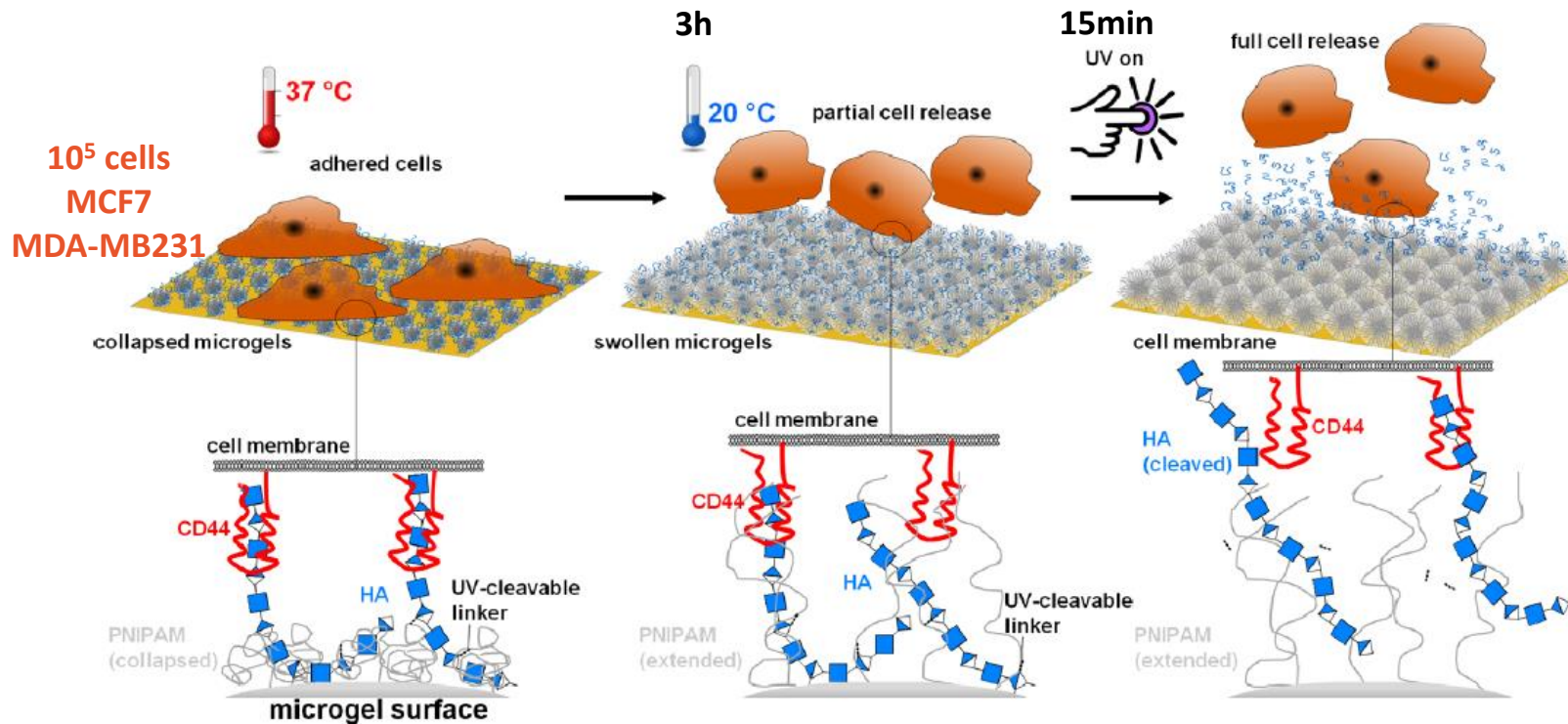


Schmidt et al., ASC Appl. Biio Mater. 2021



☒ Coating of microgels on hydrophobic silanized glass slide is homogenous and stable





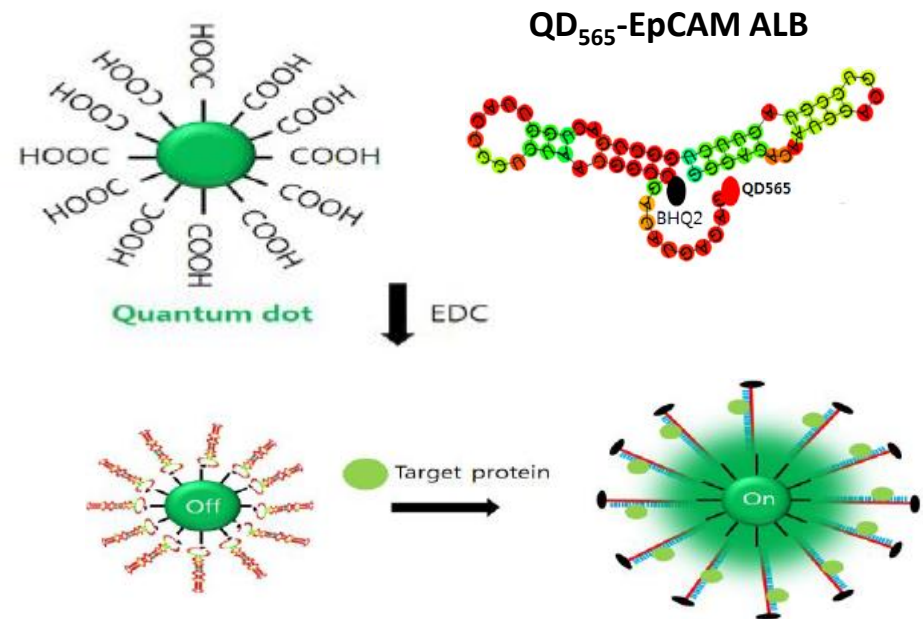
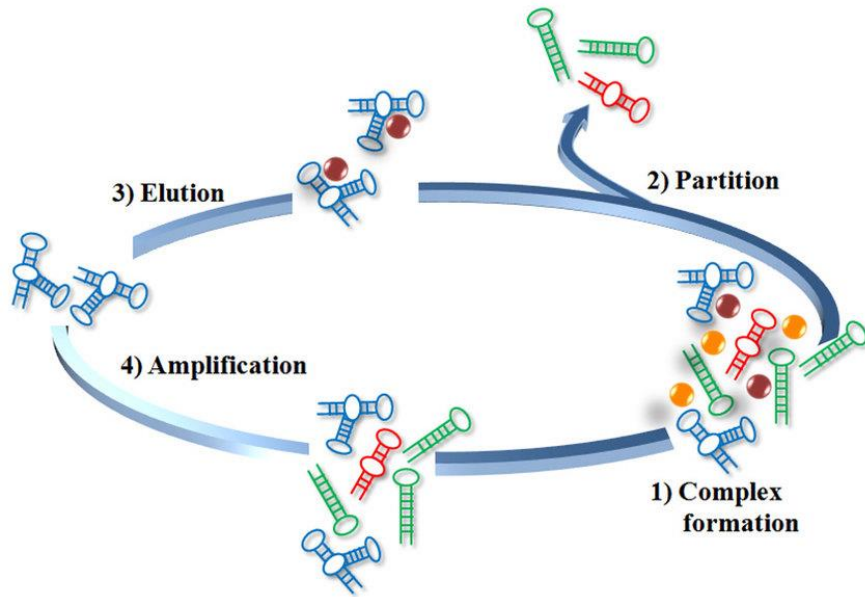
- ☒ Higher adhesion of MDA-MB-231 than MCF7 due to level of CD44 expression
- ☒ Reduced adhesion in the presence of serum proteins

- ☒ Release up to 90% of adherent cells

- ☒ Release of the remaining adherent cells

# Aptamer-based CTC detection

- Aptamer = short single strand DNA or RNA (15-100nt) interacting with various targets
- selection through SELEX (Systemic Evolution of Ligands by Exponential enrichment)

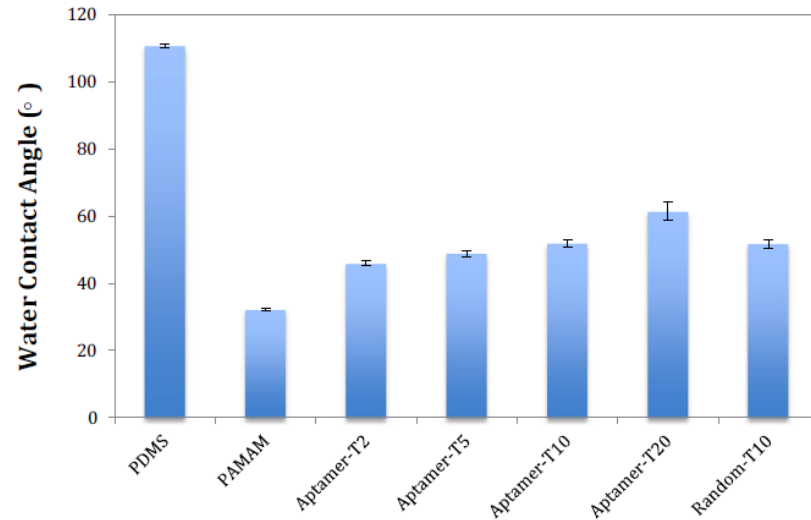
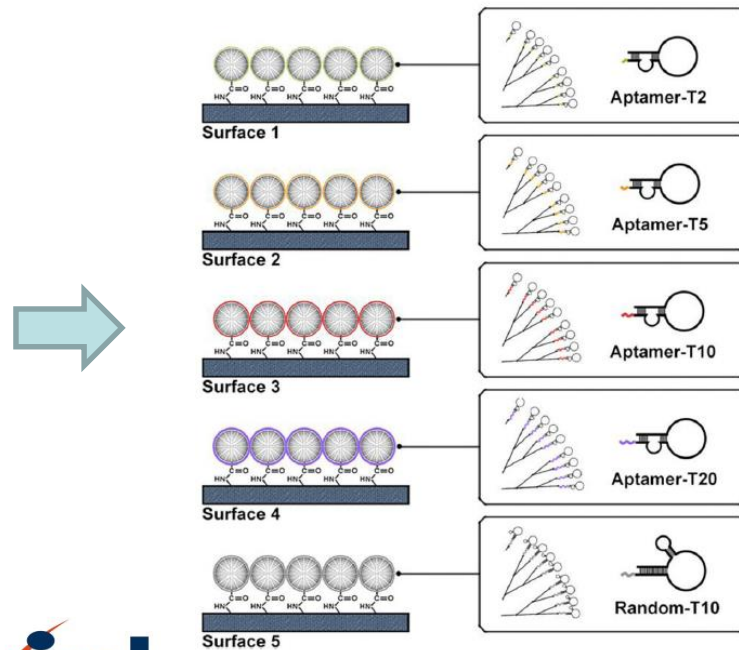
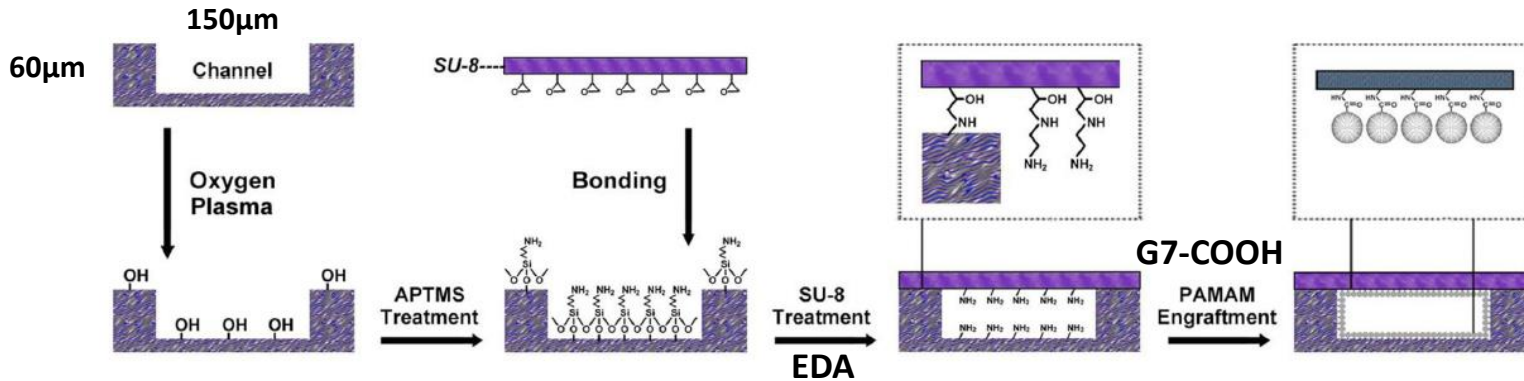


*Hwang et al., Sensors 2016*

- Fluorescence intensity of CTC in a dose-dependent response with EpCAM expression

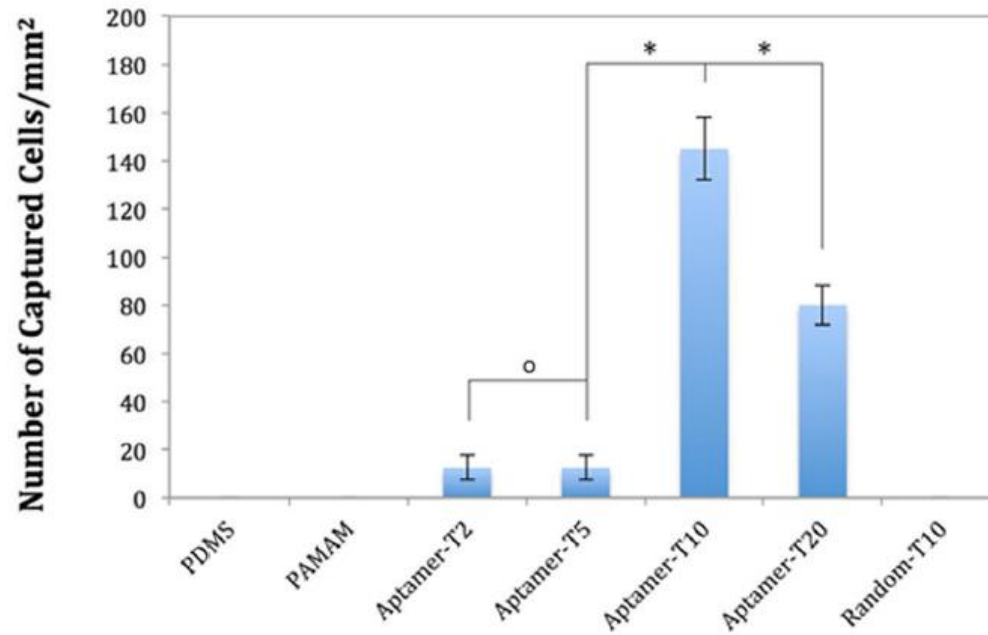
## Immobilization of aptamers into microfluidic channel

### ☒ Sgc8 aptamer specific for CCRF-CEM cells



Qin et al., Biomed Microdevices 2019

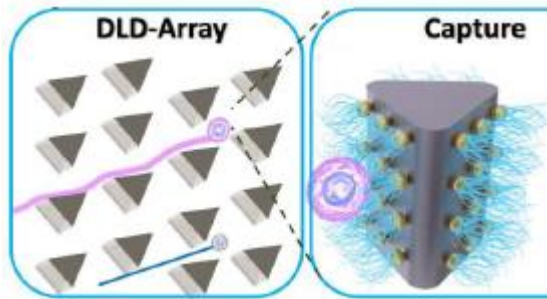
☒ Capturing performances of aptamer-functionalized surfaces by introducing  $10^6$  cells/mL at a flow rate of 0,05mL/h for 40min



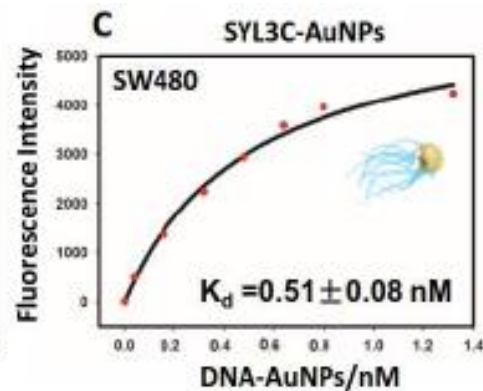
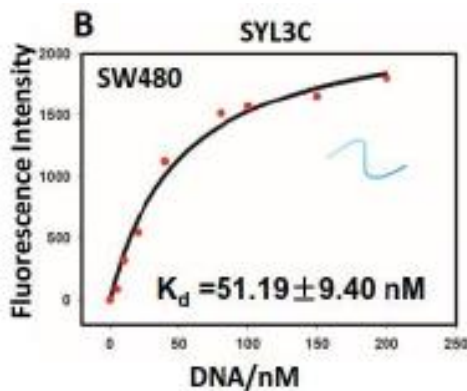
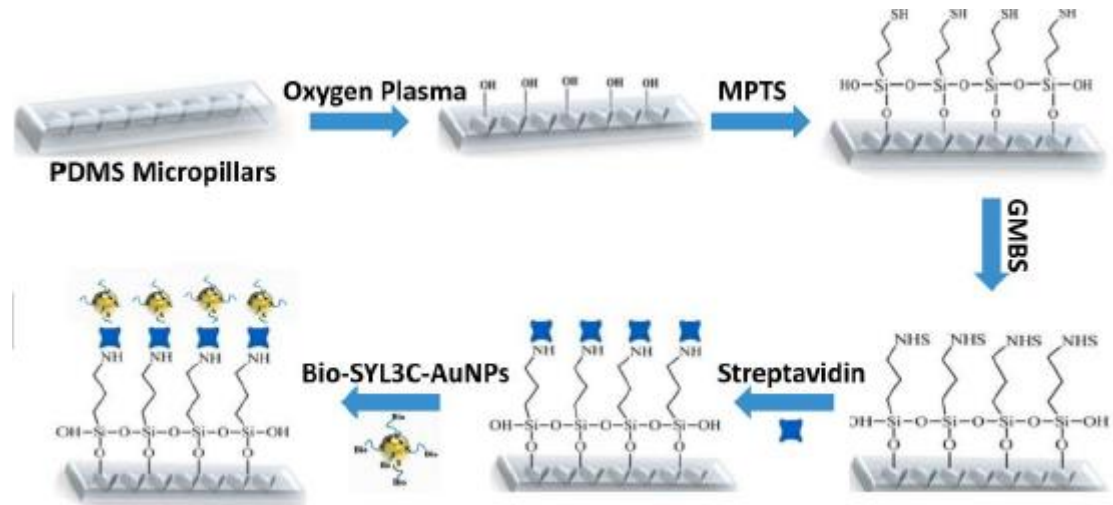
☞ Importance of the length of the spacer to improve cell capture and detection

## ☞ Multivalent aptamer Octopus Chip

Aptamer SYLC3 specific for EpCAM immobilized on AuNP (16nm)

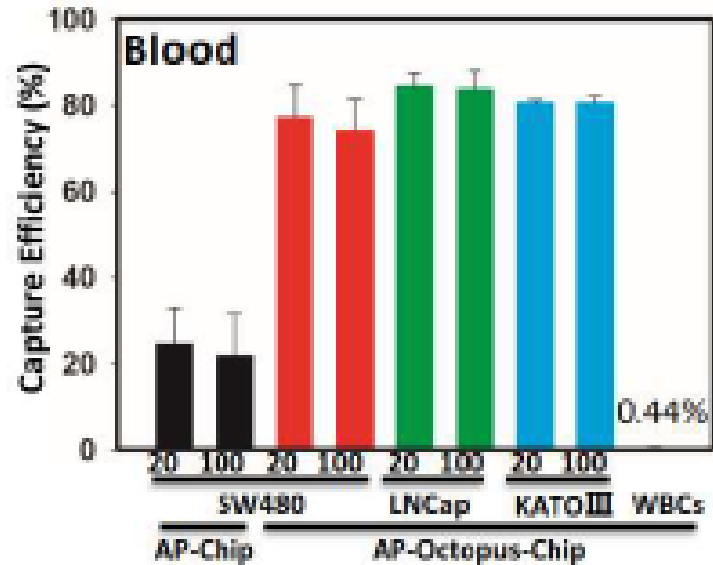
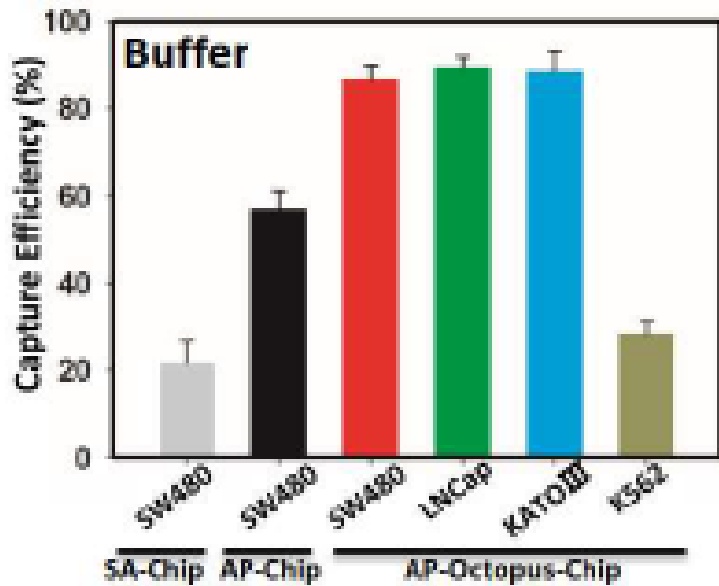


☒ Triangular micropillar increase contact time of CTC (>13 $\mu$ m) in the channel



☒ 100 times higher affinity with multivalent SYLC3-AuNP than with SYLC3 alone

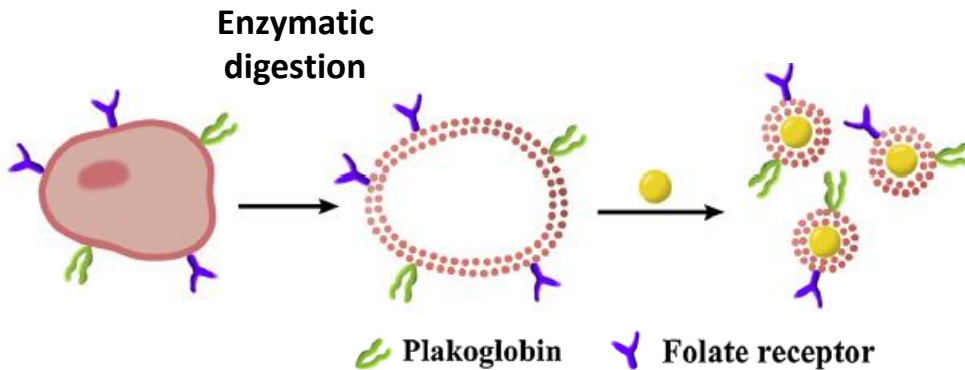
Song et al., *Angew. Chem. Inter. J.* 2019



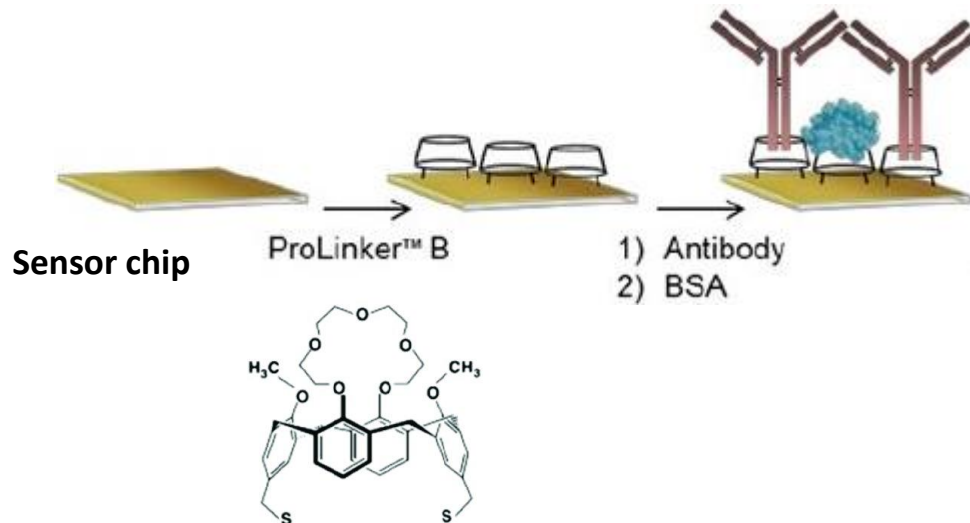
☒ Efficient and specific capture of 20-100 CTC in blood with 95% viability, and low non specific adsorption of WBC

# Membrane gold nanoparticles (M-AuNP) and SPR detection

☞ Enhancement of SPR signal with dual-selective CTC detection

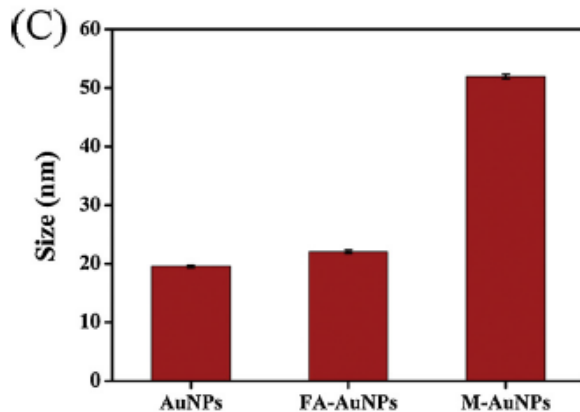
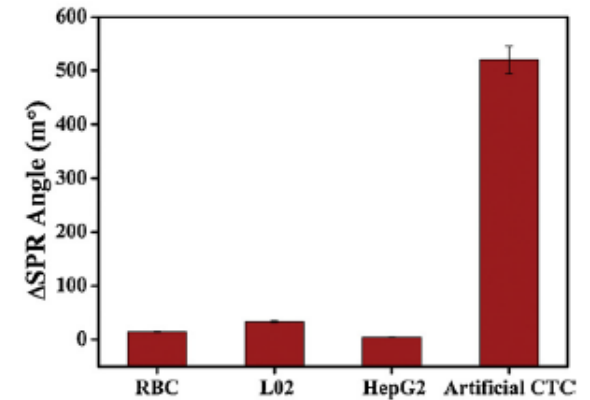
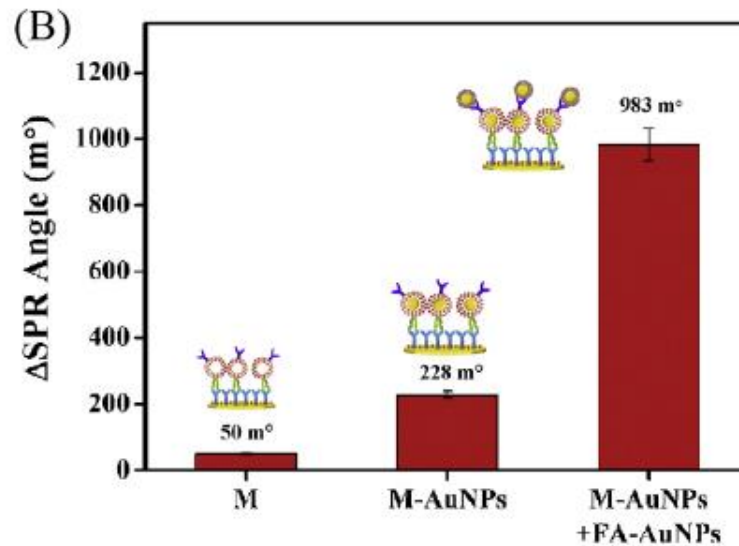
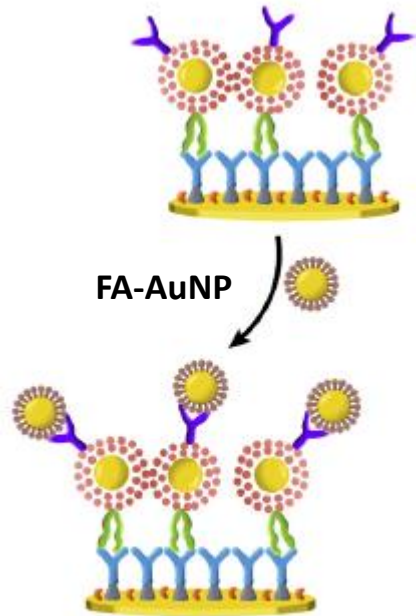


- ☒ Elaboration of M-AuNP
- ☒ Plakoglobin (JUP) is involved in desmosome junctions



- ☒ Oriented immobilisation of the anti-JUP Ab through calixarene derivative interaction

Huang et al., *Sensors and Actuators B* 2020



- ☒ The combination of JUP/anti-JUP and FA receptor/FA with AuNP increase the specificity of the detection with amplification of the signal
- ☒ Detection limit = 1 CTC/mL



# Conclusion

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- ☞ Various methods for isolating, detaching and detecting CTC have been rapidly developed
  - ☒ need to increase specificity, sensitivity and throughput
  
- ☞ Effective release of CTC from the surface after capture without damaging the cells
  - ☒ enzymatic digestion
  - ☒ aptamer-mediated release
  - ☒ stimuli-responsive polymers
  
- ☞ Many attractive advantages for microfluidic platform
  - ☒ continuous sample processing, with various functions (size, physical, electrical, marker-specific)
  - ☒ working at the cell dimension
  - ☒ But limitation due to possible clogging and low purity (physical-based), low input volume
  
- ☞ Need to establish and improve standardized protocols of CTC-related detection methods